

Harvard-MIT Division of Health Sciences and Technology

HST.535: Principles and Practice of Tissue Engineering

Instructor: Lisa E. Freed

HST 535

Principles and Practice

of Tissue Engineering

Effects of Culture Conditions

Lisa E. Freed, M.D., Ph.D.

Harvard-MIT Division of Health Sciences and Technology

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Tissue engineering approach

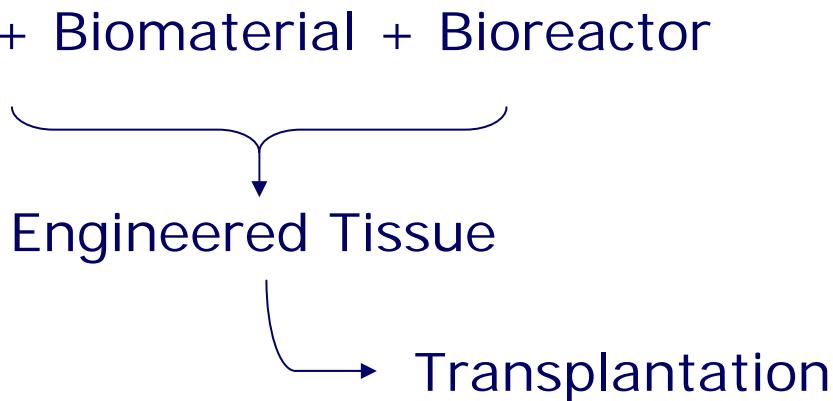
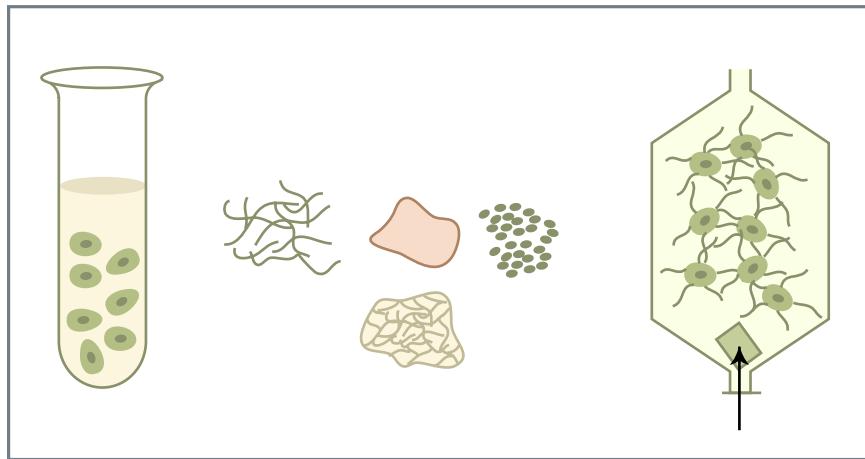


Figure by MIT OCW. After Vacanti and Langer.

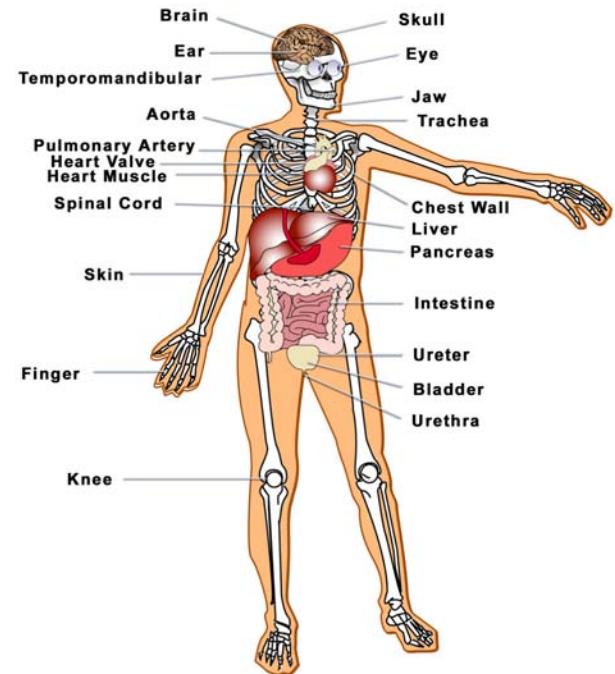


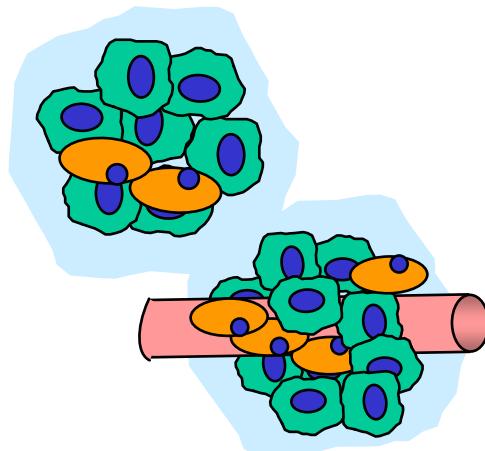
Figure by MIT OCW.

adapted from Vacanti & Langer, *Lancet* 354: 32, 1999

Culture conditions determine cell fate

- Physiological milieu (temperature , pH, oxygen)
3-dimensional environment, cell-to-cell contact)
- Biochemical factors (nutrients, growth factors)
- Physical stimulation (compression, tension)

Cell → **Differentiated Tissues**



**Loss of specialized function
senescence (aging), death**

Culture conditions key for tissue engineering

1. *Defined Culture Media*, to induce differentiation of progenitor (stem) cells.
2. *Biomaterial Scaffolds*, to provide a 3-D cell culture environment, and to influence the mechanical properties of engineered tissue.
3. *Bioreactor Vessels*, to promote spatially uniform cell seeding, and to provide mass transport and biophysical stimulation during tissue culture.

Defined media → cell differentiation

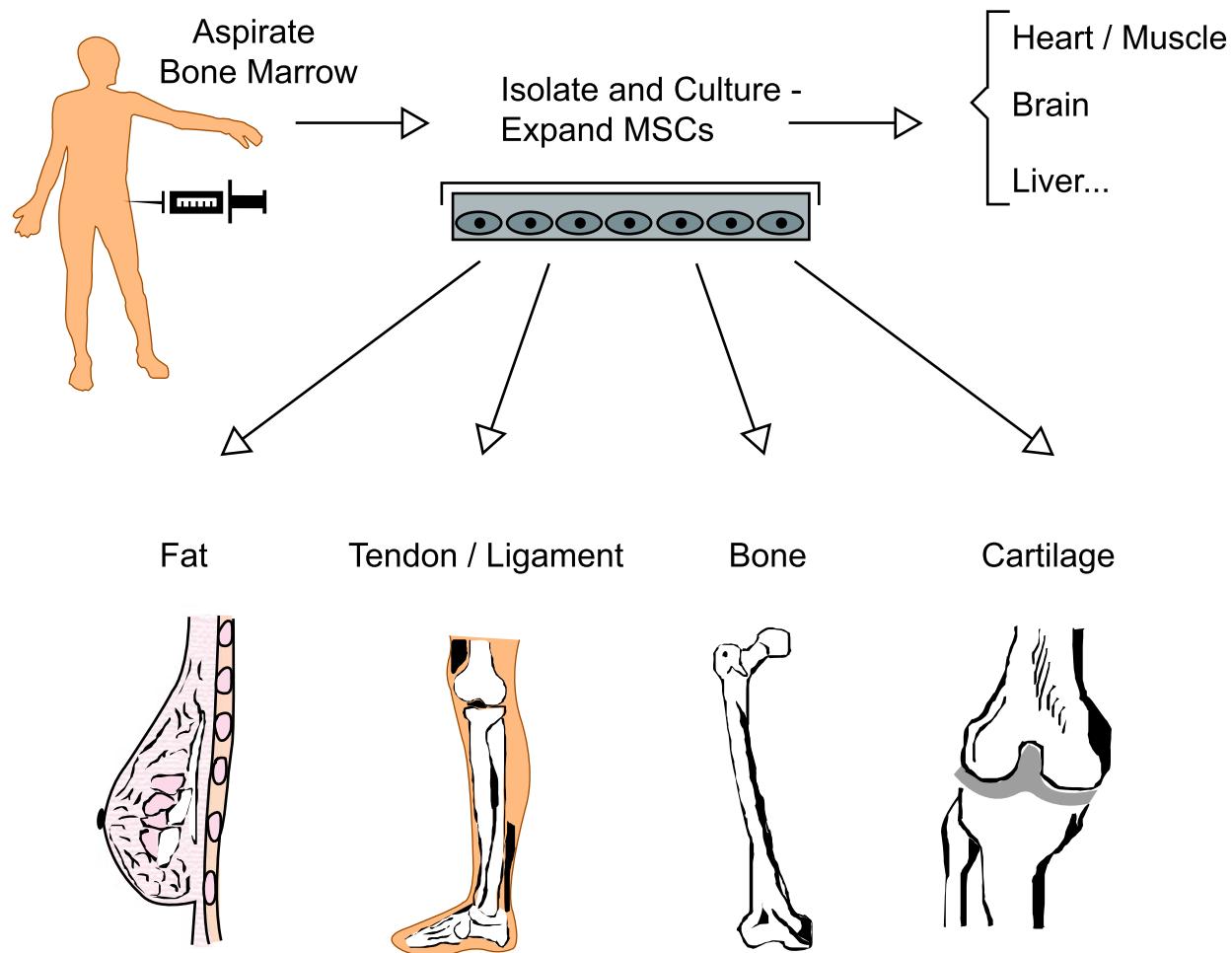
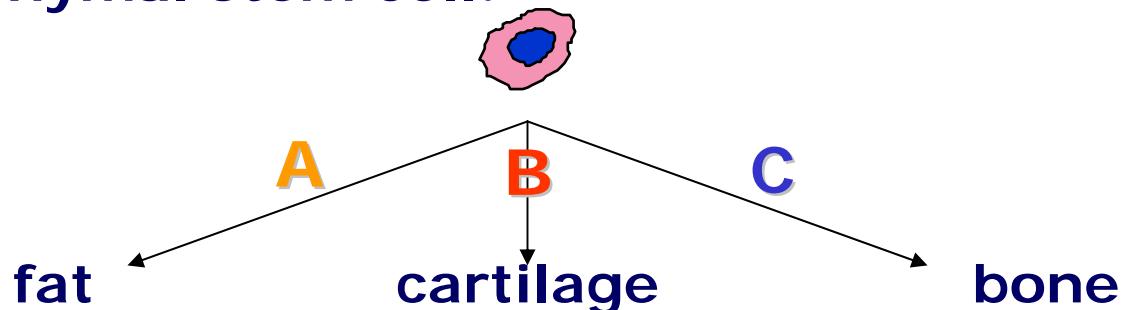


Figure by MIT OCW. After Bruder & Caplan, *Principles of Tissue Engineering*, 2000.

Medium A,B, or C → selective differentiation

mesenchymal stem cell:



donor #1

Grid of six photos removed for copyright reasons.

donor #2

Lipid Type II collagen Alkaline phosphatase

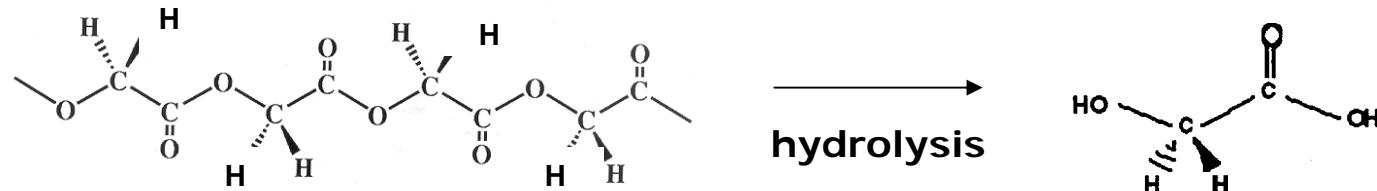
A scaffold → 3-dimensional culture (non woven mesh of polyglycolic acid, PGA)

Two photos removed for copyright reasons.

—
2 mm

—
20 µm

**Fiber diameter (13 µm) is similar to that of a cell;
Porosity is high (97 %); material is biocompatible.**



Source: Freed, L., et al. (Nat)Bio/Technol 12: 689, 1994.

3-D scaffold promoted differentiation (chondrocyte cultures)

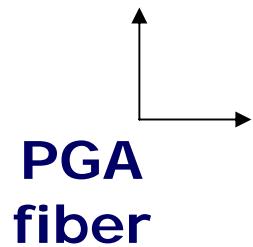


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Source: Freed, L., et al. (Nat)Bio/Technol 12: 689, 1994.

3-D scaffolds for engineering cartilage

(representative)

Three photos removed for copyright reasons.

3-D structure	sponge	non-woven mesh	woven mesh
structural stability	higher	lower	intermediate
porosity, pore inter- connectivity	lower	higher	intermediate

Appropriate biomechanics with meshes

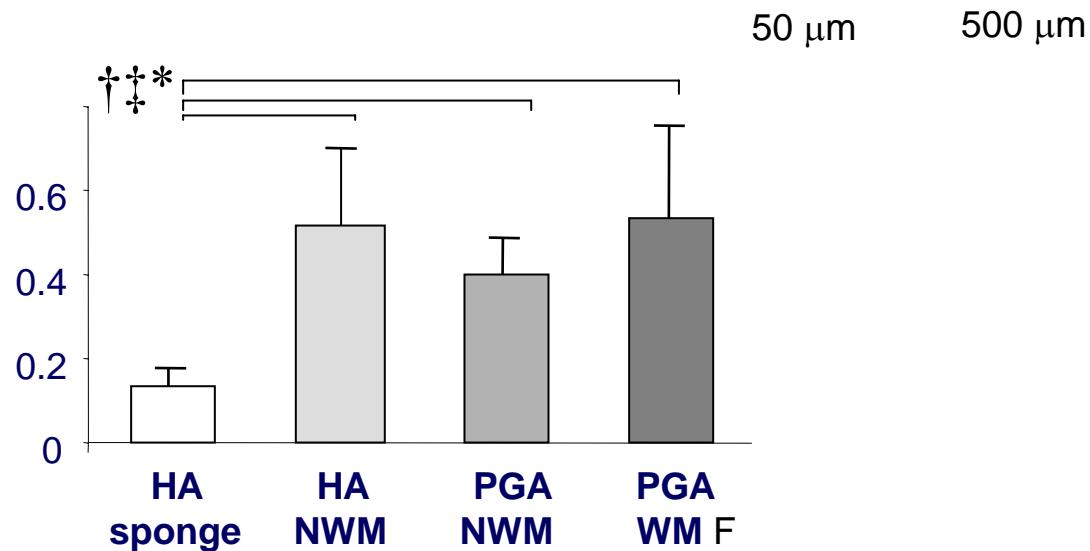
(chondrocytes on different scaffolds, 1 month)



Scaffold:

Four photos removed for copyright reasons.

Modulus (MPa)
constructs cultured
for 4 weeks



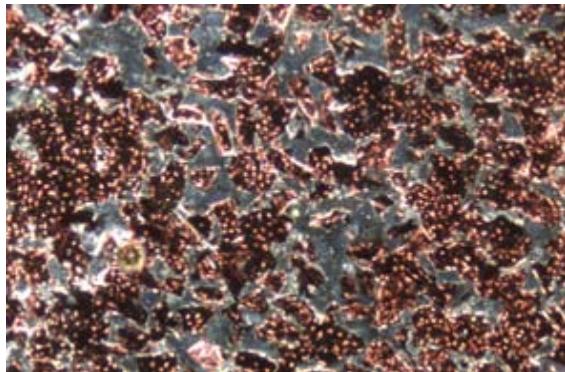
3-D cell seeding requires dynamic mixing

(chondrocytes on sponge or mesh)

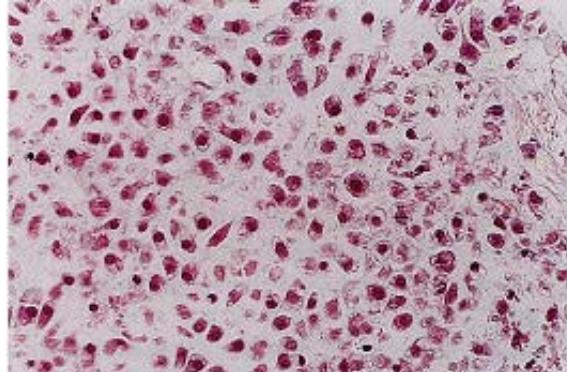
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Porous sponge:



Fibrous mesh:



3-D scaffolds for engineering heart

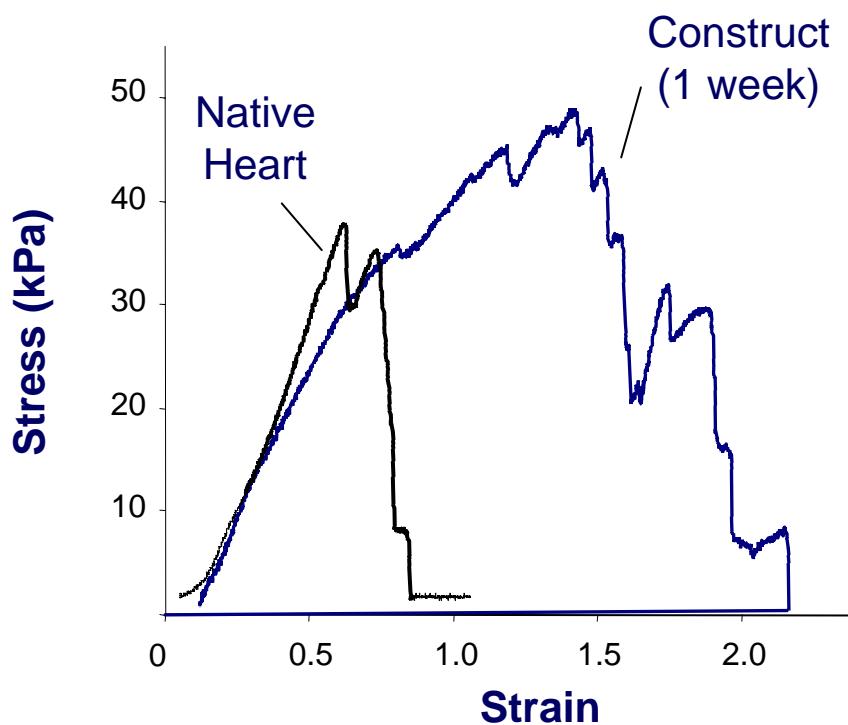
(representative)

Three photos removed for copyright reasons.

3-D structure	non-woven mesh	sponge	knitted fabric
Structural stability	low	low	high
Porosity, pore inter-connectivity	high	high	non-uniform

Appropriate biomechanics with knitted fabric

(heart cells/gel on knitted fabric, 1 week)



3D cell seeding requires hydrogel & perfusion

(C2C12 myocytes/gel on collagen sponge, 5 h)

petri dish

perfusion

Top

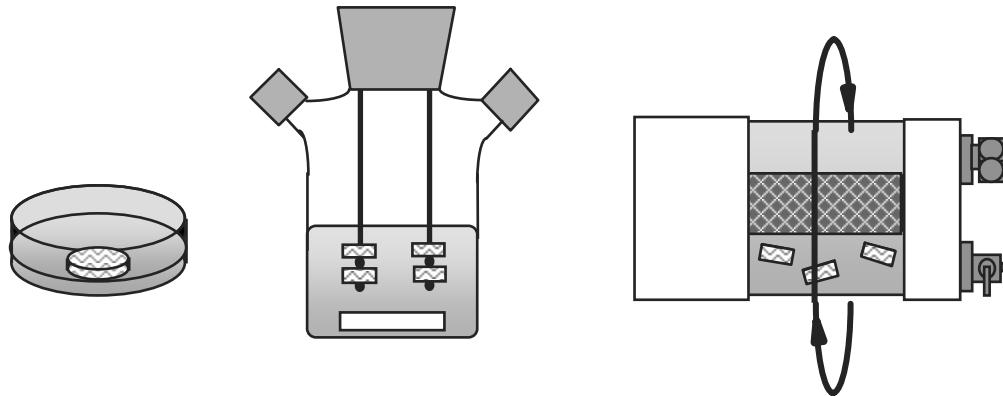
Center

Bottom

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— 100 μm

Culture systems for engineering cartilage



	static petri dish	spinner flask	rotating bioreactor
Mechanism of mixing	none	magnetic stirring	rotational flow, construct settling
Flow pattern	none	turbulent	laminar
Gas exchange	surface aeration	surface aeration	internal membrane
Mass transfer	diffusion	convection	convection

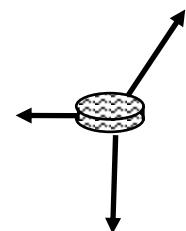
Rotating bioreactor

→ dynamic, laminar flow pattern

side view:

end view:

suspended
construct:



Images removed for copyright reasons.

Flow-visualization study and video by P. Neitzel
Freed & Vunjak-Novakovic, *Biotech Bioeng* 36: 306, 1995

Chondrogenesis in rotating bioreactor

culture day 12:

culture day 40:

Glycosaminoglycans
(safranin-O stain)

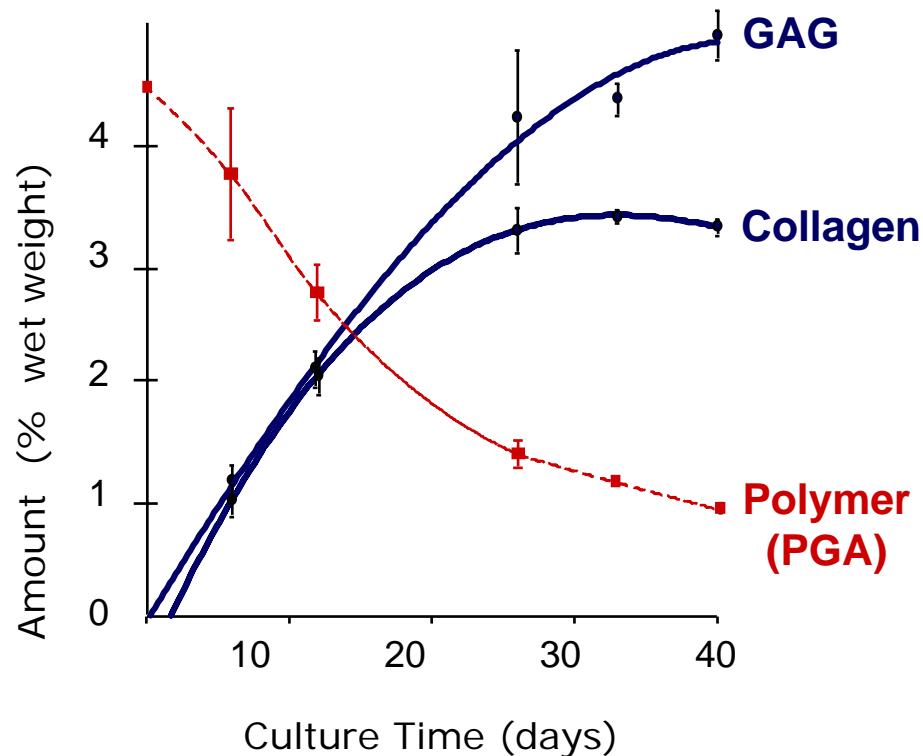
2 mm

Image removed for copyright reasons.

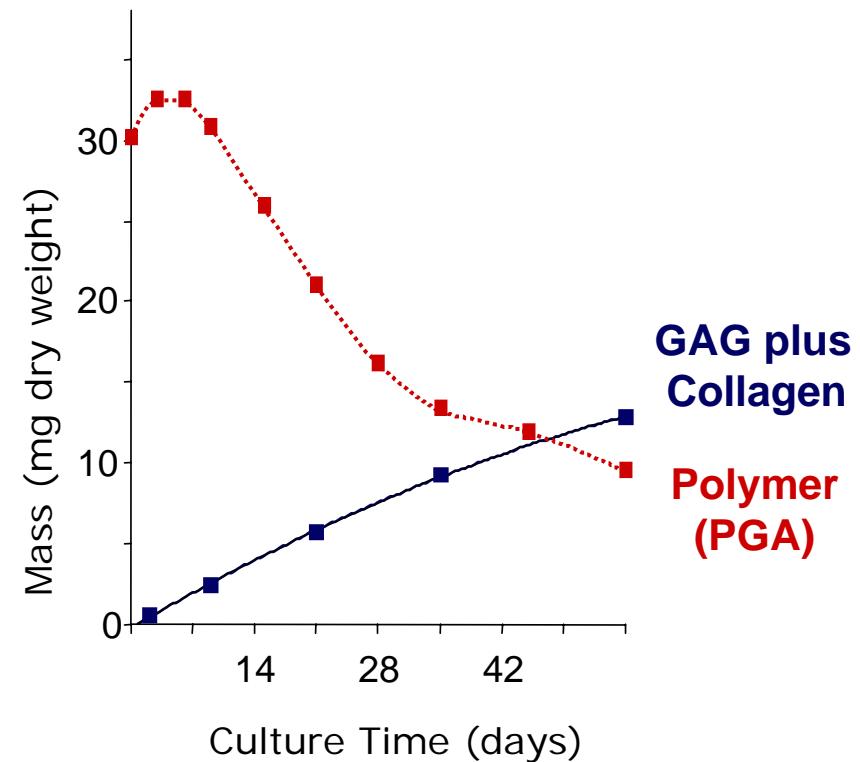
Type II Collagen
(immunostain)

Bioreactor vs. conventional culture (for chondrogenesis)

Rotating bioreactor:



Petri dish:



Bioreactors improve size and structure (engineered cartilage)



Bioreactor:

Image removed for copyright reasons.

Petri dish:

H
1 mm

Bioreactors improve molecular properties (engineered cartilage)

Bioreactor:

Petri dish:

Type I Collagen
(Western blot)

$\alpha 1/2(I)$

Image removed for copyright reasons.

Type II Collagen
(Western blot)

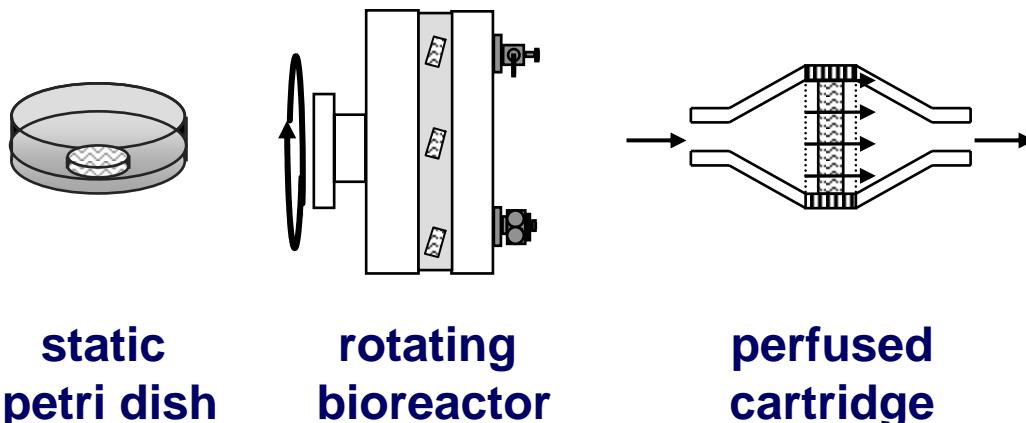
$\alpha 1(II)$

Figure 6 from Pei et al 2002.

Type I Collagen
(band intensity)

Type II Collagen
(band intensity)

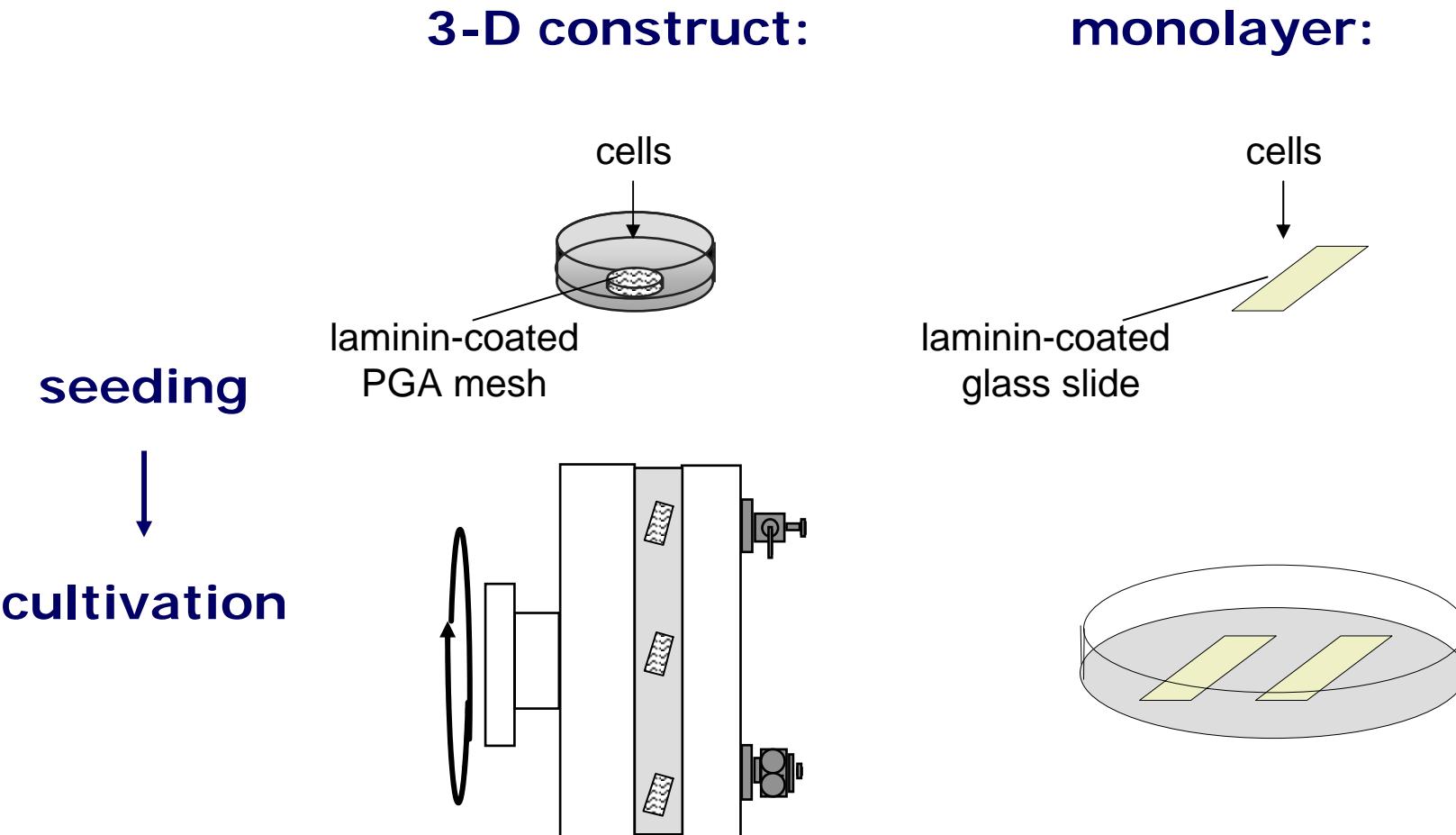
Culture systems for engineering heart



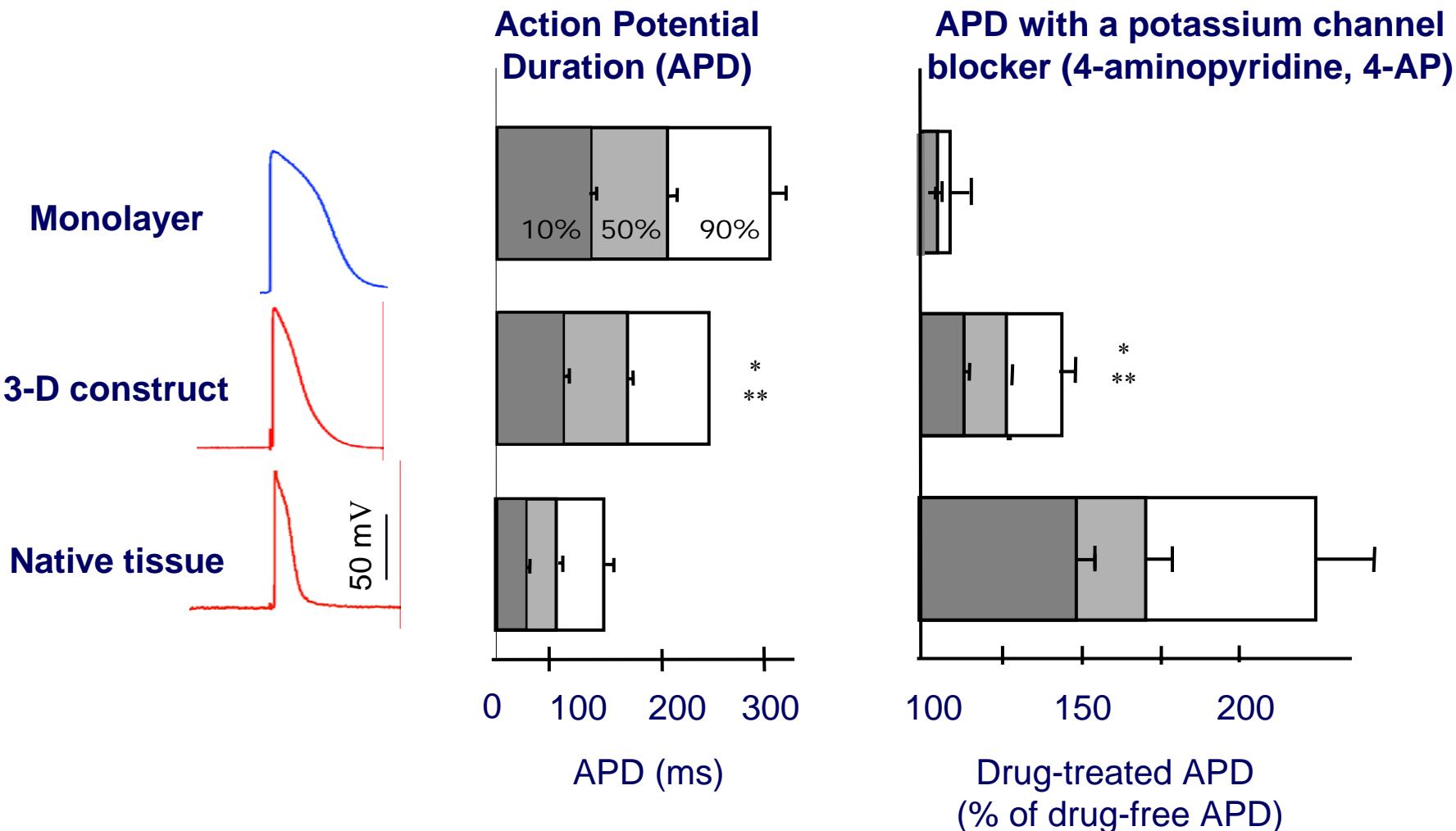
Mechanism of mixing	none	rotational flow, construct settling	recirculation of medium
Flow pattern	none	laminar	laminar
Gas exchange	surface aeration	internal membrane	external membrane
Mass transfer	diffusion	convection	convection

Controlled *in vitro* studies

(3-D construct vs. conventional culture conditions)



Appropriate electrical properties with heart cells cultured on scaffold in bioreactor



Summary

Culture conditions key for tissue engineering:

- *Defined culture media* induce cell differentiation by providing key regulatory factors
- *Biomaterial scaffolds* further enhance cell differentiation by providing a 3-D culture environment, and can influence mechanical properties of engineered tissues.
- *Bioreactors* improve cell seeding and functional tissue development by providing mixing, mass transport, and biophysical stimulation.

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